## Efficient Deterministic Compressed Sensing for Images with Chirps and Reed–Muller Codes\*

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- Abstract. A recent approach to compressed sensing using deterministic sensing matrices formed from discrete frequency-modulated chirps or from Reed–Muller codes is extended to support efficient deterministic reconstruction of signals that are much less sparse than envisioned in the original work. In particular, this allows the application of this approach in imaging. The reconstruction algorithm developed for images incorporates several new elements to improve computational complexity and reconstruction fidelity in this application regime.
- Key words. compressed sensing, Reed–Muller codes, frequency-modulated chirps, image reconstruction, medical imaging

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**1.** Introduction. In the few years since the foundational ideas of compressed sensing were set forth by Donoho [19] and Candès and Tao [15, 11], the methodology has inspired a substantial body of research seeking to exploit sparsity in various classes of signals to enable efficient measurement approaches [27, 32, 33]. While most of the emphasis has been connected with the use of stochastic measurement matrices, a few researchers have sought to develop deterministic measurement strategies. Among these is an approach introduced by Applebaum et al. [2] and extended by Howard, Calderbank, and Searle [25] in which the columns of the measurement matrix consist of sampled linear frequency-modulated chirps or the closely related second-order Reed–Muller codes. This approach includes a deterministic algorithm for reconstructing the original sparse signal from measurements that is shown to compare favorably to reconstruction methods used in other compressed sensing contexts, particularly so when the signal is extremely sparse. The performance of this algorithm deteriorates significantly, both in speed and fidelity, when the signal is less sparse. In most image processing applications, intrinsic compressibility of classes of images using a suitable basis (e.g., wavelets) typically makes high-accuracy approximation by a sparse image possible only if the sparsity is 5-20%or higher. Thus, the reconstruction algorithm for chirp compressed sensing given in [2] and the closely related algorithm for Reed–Muller compressed sensing given in [25] are not suitable

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N	dimension of the signal space
x	signal N-vector
k	sparsity of $x$
n	# of measurements
Φ	$n \times N$ measurement matrix
j	matrix column index
$\ell$	matrix row index
y	<i>n</i> -vector of measurements
A	$n \times t$ matrix formed from columns of $\Phi$ , $0 \le t \le k$
z	vector of length $t$

		Table 1		
Notation	used	throughout	this	paper.

for use with images. The primary contribution of this paper is to describe and demonstrate a reconstruction algorithm that extends the utility of compressed sensing with chirp and Reed–Muller measurement matrices into a regime of less sparsity, thereby supporting imaging applications.

Following this introductory section, the paper continues in section 2 with a synopsis of background material, focusing on the use of chirps and Reed–Muller codes in compressed sensing. Background and notation used throughout the remainder of the paper are introduced in the course of this synopsis. Section 3 is the heart of the paper. It begins by explaining the shortcomings of the reconstruction algorithms of [2] and [25] that manifest when the signal is not highly sparse. It then proceeds to describe the approach taken to extend compressed sensing with chirps and Reed–Muller codes to support imaging. Appropriate construction of the sensing matrix, with attention to satisfaction of the statistical restricted isometry property (StRIP) [8], is addressed in this section along with a description of the corresponding reconstruction algorithms for both chirp and Reed–Muller measurement matrices. In fact, three variants of the basic algorithms that incorporate various techniques for numerical implementation of the key steps are presented. Section 4 provides analytical and experimental results pertaining to the performance of the method. The paper concludes in section 5 with a brief discussion of the work presented and some thoughts regarding future directions for this vein of research.

2. Background. The essential elements of compressed sensing are rather well documented in recent research literature. The papers by Baraniuk [3] and Candès and Wakin [16], for example, present clear synopses of the basics. Consequently, this section provides only a concise description of the general compressed sensing problem to establish notation, and then presents enough background on the deterministic approaches of [2] and [25] to enable subsequent analysis of their shortcomings in imaging applications.

Table 1 summarizes notation used throughout the remainder of this paper.

**2.1. Compressed sensing.** A signal  $x \in \mathbb{C}^N$  is k-sparse in a basis  $\Psi = \{\psi_j\}_{j=1}^N$  if x is a weighted superposition of at most k elements of  $\Psi$ . Compressed sensing broadly refers to the inverse problem of reconstructing such a signal x from linear measurements  $\{y_\ell = \langle x, \phi_\ell \rangle | \ell = 1, \ldots n\}$  with n < N, ideally with  $n \ll N$ . Denoting by  $\Psi$  the  $N \times N$  matrix having the basis elements  $\psi_j$  as its columns and by  $\Phi$  the  $n \times N$  matrix having the measurement vectors  $\phi_\ell$  as

its rows yields

$$(2.1) y = \Phi x = \Phi \Psi s$$

In this expression, y is an *n*-vector of measurements and s is an *N*-vector in which at most k components are nonzero. If  $\Psi$  is known, then reconstructing x from y is equivalent to reconstructing s from measurements  $\Phi\Psi s$ . For this reason, it is common to simplify notation by assuming  $\Psi$  is the standard basis and x itself contains no more than k nonzero components. Except in a few places where the sparsifying basis  $\Psi$  is explicitly needed, this assumption will be used throughout the rest of this paper.

Much of the compressed sensing literature is concerned with conditions on the measurement matrix  $\Phi$  under which the k-sparse assumption on x regularizes, either with certainty or very high probability, the ill-posed problem of recovering it from y. An important sufficient condition in this regard is the restricted isometry property (RIP) [13], which stipulates that, for some  $\varepsilon > 0$ ,

(2.2) 
$$(1-\varepsilon)\|x\|_2^2 \leqslant \|\Phi_{\mathrm{sub}}x\|_2^2 \leqslant (1+\varepsilon)\|x\|_2^2 \qquad \forall x \in \mathbb{C}^k$$

must hold for every  $n \times k$  matrix  $\Phi_{\text{sub}}$  formed from k distinct columns of  $\Phi$ . In this expression,  $\|\cdot\|_2$  denotes the  $\ell^2$ -norm, defined by  $\|x\|_2 := (\sum_{i=1}^N |x_i|^2)^{1/2}$ . While verifying the RIP for a given measurement matrix  $\Phi$  is combinatorially complex, it has been established that certain classes of randomly generated matrices (e.g., whose entries are realized from independent Gaussian random variables) manifest the RIP with very high probability. One should note that (2.2) is equivalent to the following relation [15] between the minimum and maximum eigenvalues of the Grammian  $\Phi_{\text{sub}}^* \Phi_{\text{sub}}$ :

$$1 - \varepsilon \le \lambda_{\min}(\Phi_{\sup}^* \Phi_{\sup}) \le \lambda_{\max}(\Phi_{\sup}^* \Phi_{\sup}) \le 1 + \varepsilon.$$

As noted above, the use of randomly generated matrices has become prevalent in compressed sensing. For a Gaussian measurement matrix, reconstruction of x from y is generally possible if  $n > ck \log(N/k)$  [15, 13, 3], with reconstruction entailing a convex  $\ell_1$  optimization problem, such as

(2.3) 
$$\min \|\tilde{x}\|_1 \quad \text{such that} \quad y = \Phi \tilde{x}$$

where  $\|\tilde{x}\|_1 = \sum_{i=1}^N |\tilde{x}_i|$ . Algorithms to efficiently solve such problems have received much recent attention specifically in connection with their utility in compressed sensing [21, 34, 22, 5]. The popular basis pursuit algorithm [14] has computational complexity  $\mathcal{O}(N^3)$ ; alternatives to basis pursuit (e.g., greedy matching pursuit) also have computational complexities that depend on N.

**2.2. Statistical RIP.** In [8], Calderbank, Howard, and Jafarpour set forth criteria on  $\Phi$  that ensure a high probability that the mapping taking the k-sparse signal vector x to the measurement vector y is injective, assuming a specific probability distribution on the unit-magnitude k-sparse vectors in  $\mathbb{C}^N$ . They say that  $\Phi$  has the StRIP with respect to parameters  $\varepsilon$  and  $\delta$  if

(2.4) 
$$(1-\varepsilon)\|x\|_{2}^{2} \le \|\Phi x\|_{2}^{2} \le (1+\varepsilon)\|x\|_{2}^{2}$$

holds with probability exceeding  $1 - \delta$  when x is assumed to be uniformly distributed among k-sparse vectors in  $\mathbb{C}^N$  of some fixed norm (e.g., unit norm). They further say that  $\Phi$  has the uniqueness-guaranteed statistical restricted isometry property (UStRIP) with parameters  $\varepsilon$  and  $\delta$  if, in addition to having the StRIP for  $\varepsilon$  and  $\delta$ ,

$${\hat{x} \ k}$$
-sparse in  $\mathbb{C}^N$  :  $\Phi \hat{x} = \Phi x = {x}$ 

with probability exceeding  $1 - \delta$ .

The implication of  $\Phi$  possessing the UStRIP on recovery of x from  $y = \Phi x$  is evident. A further result in [8] provides a set of three conditions that are sufficient to establish that a matrix  $\Phi$  possesses the UStRIP. Specifically, suppose that

(p1) the rows of  $\Phi$  are orthogonal and all the row sums are zero;

(p2) the columns of  $\Phi$  form a group under "pointwise multiplication"; and

(p3) for all  $j \in \{2, \ldots, N\}$ ,  $|\sum_{\ell} \phi_j(\ell)|^2 \le n^{1-\eta}$ .

Then if  $k < 1 + (N-1)\varepsilon$  and  $\eta > 1/2$ , there exists a constant C such that, if  $n \ge (C\frac{k \log N}{\varepsilon^2})^{\frac{1}{\eta}}$ ,  $\Phi$  possesses the UStRIP with parameters  $\varepsilon$  and

(2.5) 
$$\delta = 2 \exp\left(-\frac{[\varepsilon - (k-1)/(N-1)]^2 n^{\eta}}{32k}\right).$$

The deterministic compressed sensing matrices proposed in [2, 25] and discussed in sections 2.3 and 2.4 below satisfy the UStRIP. In section 3.2 of this paper, the above criteria will be used to show that certain related deterministic matrices also have the UStRIP.

**2.3. Compressed sensing with chirps.** Applebaum et al. [2] proposed and demonstrated a deterministic compressed sensing scheme using matrices of discrete "chirps," i.e., frequency-modulated discrete sinusoids. Specifically, a discrete chirp of length n with *chirp rate* r and *base frequency* m has the form

(2.6) 
$$\phi_{r,m}(\ell) = \frac{1}{\sqrt{n}} e^{\frac{2\pi i}{n} r \ell^2 + \frac{2\pi i}{n} m \ell}, \qquad r, m, \ell \in \mathbb{Z}_n.$$

Note that the coefficient  $1/\sqrt{n}$  is present in order for the vector to have a unit  $\ell_2$ -norm. For a fixed *n*, there are  $n^2$  possible pairs (r, m). The full chirp sensing matrix  $\Phi$  thus has size  $n \times n^2$  and can be written as

(2.7) 
$$\Phi_{\text{chirp}} = \begin{bmatrix} U_{r_1} & U_{r_2} & \cdots & U_{r_t} & \cdots & U_{r_n} \end{bmatrix}, \quad 1 \le t \le n.$$

Each  $U_{r_t}$  is an  $n \times n$  matrix with columns given by chirp signals having a fixed chirp rate  $r_t$  with base frequency m varying from 0 to n-1. The chirp rate r also varies from 0 to n-1. Therefore, column j = m + rn + 1 of  $\Phi_{chirp}$  is a discrete chirp with chirp rate r and base frequency m. In [2], the suitability of  $\Phi_{chirp}$  for compressed sensing was demonstrated empirically by comparing the eigenvalues of the Grammians of matrices consisting of k columns chosen uniformly at random from the chirp matrix with those from Gaussian matrices. In [8],  $\Phi_{chirp}$ was shown to possess the UStRIP. To do so, each submatrix  $U_{r_t}$  was multiplied by a unitmagnitude scalar  $e^{\frac{2\pi i}{n}r_t}$  to achieve the row-sum condition described in the preceding section.

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A key advantage of compressed sensing with chirp matrices is that it admits a fast reconstruction algorithm whose complexity,  $\mathcal{O}(kn^2 \log n)$  (see [2]) versus  $\mathcal{O}(knN)$  for basis pursuit with matching pursuit, depends only on the number of measurements n and not on the signal length N. This algorithm and a closely related one for reconstruction from compressed measurements made with Reed–Muller matrices are discussed further in section 2.5.

**2.4. Reed–Muller (RM) sensing matrix.** In [25], Howard, Calderbank, and Searle introduced the idea of deterministic compressed sensing using a matrix of real-valued second-order RM codes [28]. In the construction summarized in [8], based on [17, 23], the set of such codes with length  $2^p$  is parameterized by  $p \times p$  binary symmetric matrices P and binary p-vectors  $b \in \mathbb{Z}_2^p$ . In terms of these parameters, a second-order RM code is given by

(2.8) 
$$\phi_{P,b}(a) = \frac{1}{\sqrt{2^p}} i^{(2b+Pa)^{\mathsf{T}}a}.$$

In this expression,  $a \in \mathbb{Z}_2^p$  indexes the  $2^p$  components of the code  $\phi_{P,b}$ . So, for given parameters P and b, the code is a vector of length  $2^p$ . These vectors will serve as the columns of the sensing matrix  $\Phi_{\text{RM}}$ . In addition, P is assumed to be zero on its main diagonal throughout this paper. This implies that the components of these codes are all  $\pm 1$ , and the codes obtained under this assumption are the same as would be obtained by generating complex codes of length  $2^{p-1}$  and applying the Gray map [23]. The compressed sensing matrix proposed in [25] has the form

(2.9) 
$$\Phi_{\rm RM} = \begin{bmatrix} U_{P_1} & U_{P_2} & \cdots & U_{P_t} & \cdots & U_{P_{2^{p(p-1)/2}}} \end{bmatrix}, \quad 1 \le t \le 2^{p(p-1)/2},$$

where each  $U_{P_t}$  is a  $2^p \times 2^p$  orthogonal matrix whose columns are  $\phi_{P_t,b}$  with b going through all binary p-vectors. In addition, each  $\phi_{P,b}$  is multiplied with a phase factor  $(-1)^{\text{wt}(b)}$ , where wt(b) is the Hamming weight of b, i.e., the number of ones in b. The extra phase factor ensures that the total number of plus and minus signs of the inner products of any two columns are the same. For convenience,  $P_1$  is chosen to be the zero matrix, and therefore, without the phase factor,  $U_{P_1}$  is a Hadamard matrix up to a scaling [24]. Consequently, multiplication by  $U_{P_1}$  is the Walsh–Hadamard transform which, up to a scaling, is its own inverse [24]. In this paper, the scalings are chosen so that each column in  $\Phi_{\text{RM}}$  has unit norm.

In analogy with chirps, the vector b in the linear term of (2.8) and the matrix P in the quadratic term may be regarded as the "frequency" and "chirp rate" of the code, respectively. Useful insight about the structure of this collection of codes arises from considering the structure of the set of  $p \times p$  binary symmetric matrices. First, there are  $2^{p(p-1)/2}$  such matrices with zero-diagonal, so the maximum size of the RM sensing matrix is  $2^p \times 2^{p(p+1)/2}$ . This is substantially larger than the chirp matrix discussed in the previous section. For a given P,  $2^p$  codes are obtained by varying b, and normalizing them to unit length yields the columns of a  $2^p \times 2^p$  unitary matrix. The Delsarte–Goethals set DG(p, r) is the binary vector space of  $p \times p$  binary symmetric matrices with the property that the difference between any two distinct matrices has rank greater than or equal to p - 2r [23]. Evidently these sets are nested as follows

$$DG(p,0) \subset DG(p,1) \subset \cdots \subset DG\left(p,\frac{p-1}{2}\right).$$

Restricting the matrices P to reside in DG(p, 0) produces the Kerdock codes [26]. Two distinct Kerdock codes, normalized to unit length, have inner product modulus that is either zero (if they correspond to the same P) or  $1/\sqrt{2^p}$  (if they correspond to distinct P). More generally,

(2.10) 
$$|\langle \phi_{P,b}, \phi_{P',b'} \rangle| = \begin{cases} \frac{1}{\sqrt{2^q}}, & 2^q \text{ times,} \\ 0, & 2^p - 2^q \text{ times,} \end{cases}$$

where  $q = \operatorname{rank}(P - P')$ . So, if the domain of P is DG(p,q), the set of possible inner product modulus values for distinct normalized codes is  $\{0, 2^{-p/2}, \ldots, 2^{-(p-2r)/2}\}$ . Allowing P to range over all of DG(p, (p-1)/2), (2.8) gives the full set of second-order RM codes.

Defining  $N = 2^{p(p+1)/2}$  and  $n = 2^p$ , a k-sparse signal  $x \in \mathbb{C}^N$  yields a measurement  $y = \Phi_{\text{RM}} x \in \mathbb{C}^n$ , which is the superposition of k RM functions

(2.11) 
$$y(a) = z_1 \phi_{P_1, b_1}(a) + z_2 \phi_{P_2, b_2}(a) + \dots + z_k \phi_{P_k, b_k}(a) = \sum_{t=1}^k z_t \phi_{P_t, b_t}(a)$$

In (2.11),  $z_t$  are used instead of x in order to write only the nonzero terms, and  $P_t$  and  $b_t$  may individually repeat in the equation.

Comparisons between the condition numbers of the Grammians of randomly selected kcolumn submatrices of the RM matrix and of Gaussian matrices, shown in [25], indicate empirically that the average condition numbers are indistinguishable. This evidence supports their utility as compressed sensing matrices, despite the observation that they almost certainly do not have the RIP. In [8], compressed sensing matrices formed from RM codes were shown to have the UStRIP.

**2.5.** Quadratic reconstruction algorithm. A key advantage of compressed sensing with chirps and RM codes is that they admit fast deterministic reconstruction algorithms that perform very well for highly sparse signals. These algorithms, which are closely related, are summarized here to support discussion in section 3 about how their performance can be improved when the signals to be reconstructed are less sparse.

To recover the sparse signal x from the chirp measurement vector y, Applebaum et al. [2] used a fast Fourier transform (FFT) based algorithm to identify the  $(r_t, m_t)$  values corresponding to the locations of the nonzero components of x. The total computational complexity of identifying all k nonzero locations is  $\mathcal{O}(kn^2 \log n)$ . The magnitudes  $z_t$  of the nonzero components are found by solving an associated least-squares problem. In summary, their chirp reconstruction algorithm repeats the following steps. Initially, let  $y_0 = y$  be the measurement; then after an iteration of the following algorithm,  $y_0$  will denote the residual of the measurement.

Algorithm for signal reconstruction via chirp sensing matrix.

For  $t = 1, 2, 3, \ldots$ 

- 1. For each  $T \neq 0$ , calculate  $w_T$  = the peak location of FFT{ $\overline{y_0(\ell)}y_0(\ell+T)$ }. Find  $r_t$  by solving  $w_T = 2r_t T \pmod{n}$ .
- 2. Let  $m_t$  = the peak location of FFT  $\left\{ y_0(\ell) e^{-\frac{2\pi i r_t \ell^2}{n}} \right\}$ . 3. Determine  $z_l$  by minimizing  $\|y_0(\ell) \sum_{l=1}^t z_l e^{\frac{2\pi i r_l \ell^2}{n} + \frac{2\pi i m_l \ell}{n}} \|_2$ .

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4. Define  $y_0(\ell) = y_0(\ell) - \sum_{l=1}^t z_l e^{\frac{2\pi i r_l \ell^2}{n} + \frac{2\pi i m_l \ell}{n}}$ . Terminate if  $||y_0||_2$  is sufficiently small. Step 1 finds the chirp rate associated with the nonzero location having the largest coefficient. Multiplication of a shifted replicate of  $y(\ell + T)$  with its conjugate  $\overline{y(\ell)}$  results in the chirp rates appearing linearly rather than quadratically in the complex exponentials, and thus chirp rates are mapped to frequency components by the FFT in step 1. Note that for step 1 to work properly, n has to be a prime number to uniquely determine  $r_t$ . Moreover, all  $T = 1, \ldots, n-1$  are used to enhance robustness to noise and cross-term interference that is problematic with less sparse data. Once the chirp rate of the largest peak is found, step 2 dechirps the measurement and then applies the FFT to find the frequency associated with the peak. In step 3, the values of the nonzero coefficients are found by solving a leastsquares problem. Finally, the residual is computed before detecting the next largest peak. According to [2], this algorithm is more efficient than matching pursuit with random matrices for sufficiently sparse signals.

With the RM sensing matrix, the fast Walsh-Hadamard transform (FHT) is used to detect the nonzero locations,  $(P_t, b_t)$  pairs. The total computational complexity of this reconstruction is  $O(kn(\log n)^2)$ . Initially, let  $y_0 = y$  be the residual measurement. In this case, the quadratic reconstruction algorithm repeats the following steps until the residual  $y_0$  is small.

Algorithm for signal reconstruction via RM sensing matrix.

For  $t = 1, 2, 3, \ldots$ 

- 1. For each  $e_i$ , i = 1, ..., p, calculate  $w_i$  = peak location of FHT $\{y_0(a)y_0(a + e_i)\}$ . The *i*th column of  $P_t$  is the  $w_i$ th element in  $\mathbb{Z}_2^p$ .
- 2. Let  $b_t = w$ th element in  $\mathbb{Z}_2^p$ , where  $w = \tilde{\text{peak}}$  location of  $\text{FHT}\{y_0(a)\overline{\phi_{P_t,0}(a)}\}$ .
- 3. Determine  $z_l$  by minimizing  $||y_0(a) \sum_{l=1}^t z_l \phi_{P_l, b_l}(a)||_2$ .

4. Define  $y_0(a) = y_0(a) - \sum_{l=1}^j z_t \phi_{P_l, b_l}(a)$ . Terminate if  $||y_0||_2$  is sufficiently small.

The idea of this algorithm is similar to the one for chirps. The most intricate part is to form the P matrix in the first step, which is a scalar in the case of the chirp matrix. For reconstructing sparse signals, in terms of reconstruction speed and fidelity, this method is also more efficient than matching pursuit with random matrices; see [8].

**3.** Approach. Despite the success for accurate reconstruction of very sparse one-dimensional (1D) signals with the algorithm described in section 2.5, application to real two-dimensional (2D) images is impractical. This is because, in general, real images are not as sparse in any transform domain as the 1D signals used in [2] or [25]. For instance, for good reconstruction of a chirp signal of length  $N = 67^2$  using n = 67 measurements, the sparsity is around k = 8. The sparsity for successful reconstruction of an RM signal of length  $N = 2^{55}$  with  $n = 2^{10}$  measurements is around k = 20. If sparsity is much larger than considered in these examples, then reconstruction is not guaranteed and the errors become very large.

A good approximation of a  $256 \times 256$  pixel image is typically obtained by retaining the largest 10% of the wavelet coefficients in some suitably chosen wavelet domain. In particular, many medical images are well approximated by transform coding using 10–20% of their wavelet coefficients but begin to show appreciable degradation as the percentage of coefficients retained falls below these levels. However, a  $256 \times 256$  image with 10% sparsity has 6,554 nonzero coefficients, which is much larger than the sparsity considered for the 1D signals in [2] and [25]. A rule of thumb (see [4, Theorem 1]) for the number of measurements in the standard

compressed sensing using the Gaussian random matrices with  $\ell_1$  minimization is given by

(3.1) 
$$n > k \log_2(1 + N/k).$$

This rule guarantees successful reconstruction with high probability if the number of measurements n is large compared to the sparsity and signal size. Using (3.1) in the above example, at least 22672 measurements are needed for the correct reconstruction. The ratio N/n is 2.89, and this implies that roughly only three chirp rates or P matrices are needed to form the sensing matrix. Therefore, the efficiency of finding nonzero locations and their coefficients using quadratic reconstruction algorithm is not fully utilized.

This section continues by describing the construction of sensing matrices adapted to the 2D case in section 3.1. Section 3.2 shows that these matrices satisfy the UStRIP. Section 3.3 explains the *first new feature* introduced in this paper: detection of the "bulk" of a signal in the first step of the approximation. This step is termed "initial best approximation," since it precedes the iteration process entailed in the two algorithms summarized in section 2.5. It is both fast and valuable to make an initial approximation that resembles a low-pass filtered version of the signal. The *second new feature* introduced here detects several (largest) peaks at once, thus significantly decreasing processing time. This is described in section 3.4. A *third innovation* is in the least-squares step and is described in sections 3.5 and 3.6. Finally, we demonstrate how these new features are combined in the numerical implementation and compare the improvement of each step in section 3.7.

**3.1.** Construction of an effective sensing matrix for image reconstruction. As explained above, due to the nature of sparsity of images and the rule of thumb (3.1), a few submatrices of  $\Phi_{chirp}$  or  $\Phi_{RM}$  can be used as the sensing matrix, with the ratio N/n = 2.89 for 10%-sparse images. In practice, a larger ratio can be used, such as 4 for 10%-sparse images, which will be analyzed later. Consequently, there is more freedom in the choice of the chirp rates, r or P matrices, when constructing the sensing matrices.

*Construction of the chirp sensing matrix.* The inner product of any pair of distinct chirp vectors is as follows:

(3.2) 
$$\left|\left\langle\phi_{r_t,m_t},\phi_{r_{t'},m_{t'}}\right\rangle\right| = \begin{cases} \frac{1}{\sqrt{n}} & \text{if } r_t \neq r_{t'}\\ 0 & \text{if } r_t = r_{t'} \text{ and } m_t \neq m_{t'}. \end{cases}$$

Therefore, a submatrix should use as few chirp rates as possible, and the choice of the chirp rates can be arbitrary. For example, the submatrix can be

(3.3) 
$$\Phi_{\rm chirp} = \begin{bmatrix} U_{r_1} & U_{r_2} & U_{r_3} & \widetilde{U}_{r_4} \end{bmatrix},$$

where  $r_1 = 0$ ,  $r_2 = 1$ ,  $r_3 = 2$ ,  $r_4 = 3$ , and  $\tilde{U}_{r_4}$  denotes a submatrix of  $U_{r_4}$  so that the column number of  $\Phi_{\text{chirp}}$  matches the signal size. When only the first J submatrices  $U_{r_1}, \ldots, U_{r_J}$  are used to form the sensing matrix, it follows from an argument given by Alltop [1, section IV] that n need not necessarily be prime. Rather the crucial condition for unique identification of the chirp rate  $r_t$  in the reconstruction algorithm given in section 2.5 is that the smallest prime divisor of n is greater than J. For instance, the sensing matrix for a 256 × 256 (N = 65536) image may be taken to be of size  $n \times N = 16385 \times 65536$ . Note that  $16385 = 5 \times 29 \times 113$  is closest to and larger than  $25\% \times 65536 = 16384$ , whose smallest prime divisor is greater than 4. Here, the 25% ratio comes from the fact that four chirp rates are used. In this example,  $\tilde{U}_{r_4}$  is of size  $16385 \times 16381$  and can be  $U_{r_4}$  without the last four columns.

Construction of the RM sensing matrix. When forming a sensing matrix from submatrices of the RM matrix, the choice of the submatrix cannot be arbitrary. The inner product of two columns of  $\Phi_{\rm RM}$ , one taken from  $U_{P_t}$  and another from  $U_{P_{t'}}$ ,  $t \neq t'$ , is given by (2.10) with  $q = \operatorname{rank}(P_t - P_{t'})$ . If q = p, the inner product is always  $1/\sqrt{2^p}$ , which is smaller than the inner product in other cases, q < p. Since the nonzero locations of the signal are unknown, it is desirable that the inner products between any two columns are as small as possible, thus making the columns of the resulting sensing matrix close to orthogonal. Taking q = p and thus drawing P matrices only from DG(p, 0) (i.e., the Kerdock set) gives the best situation. There are  $2^{p-1}$  zero-diagonal elements in the Kerdock set. More details about the Kerdock set can be found, for instance, in [7]. For instance, a sensing matrix can be constructed in the form

(3.4) 
$$\Phi_{\mathrm{RM}} = \begin{bmatrix} U_{P_1} & U_{P_2} & U_{P_3} & U_{P_4} \end{bmatrix},$$

where  $P_1, P_2, P_3$ , and  $P_4$  are matrices from the Kerdock set. For example, the sensing matrix for a 256 × 256 ( $N = 2^{16}$ ) image with 10% sparsity is of size  $n \times N = 2^{14} \times 2^{16}$ , which means that only 25% of the signal entries are sampled. Note that for images with sparsity much smaller than 10%, fewer measurements are needed, and therefore, more chirp rates or P matrices can be used, since the ratio N/n becomes larger.

**3.2. UStRIP.** This section presents a proof that the chirp and RM submatrices in section 3.1 satisfy the UStRIP. This is achieved by modifying the proof of Theorem 2.3 in [8], which guarantees the UStRIP for a class of deterministic matrices. The proof of UStRIP for these matrices proceeds in two steps. First, the expectation of  $||\Phi x||^2$  is shown to be close to  $||x||^2$ . Then, a modification of McDiarmid's inequality gives an upper bound on the probability that a multivariate function deviates within a fixed range from its expected value. The random variables of the multivariate function in the modified McDiarmid's inequality are distinct instead of independent because they are associated with the nonzero locations, which do not repeat. In [8], the proof for deterministic matrices satisfying the sufficient condition of the modified McDiarmid's inequality relies only on property (**p3**) in section 2.2 and  $k \ll N$ , and thus, can be extended to submatrices. For the first part, the following lemma is shown in [8].

Lemma 3.1. For  $\pi$ , a random permutation of N elements,

(3.5) 
$$\left(1 - \frac{k-1}{N-1}\right) \|x\|_2^2 \le \mathsf{E}_{\pi} \left[\|\Phi x\|_2^2\right] \le \left(1 + \frac{1}{N-1}\right) \|x\|_2^2.$$

The proof is based on (p1)-(p3) in section 2.2.

For the submatrices used in this paper, (p1) and (p2) are not satisfied, and thus, (3.5) is not directly implied. Therefore, what is needed is a similar inequality for submatrices. As discussed in [8], a submatrix constructed by randomly choosing columns from the full deterministic matrix can be used in compressed sensing for signals with large sparsity. However, this does not guarantee that the submatrix satisfies the UStRIP, and the associated reconstruction algorithm may not be optimally efficient. Instead, the submatrices used in this paper

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are of the form (3.3) and (3.4), which use a few chirp rates r or P. Denote the submatrix as  $\Phi = \begin{bmatrix} U_1 & -U_2 & U_3 & -U_4 \end{bmatrix}$ , where presence of the extra minus signs (or phase factors) ensures that the row sums of  $\Phi$  equal zero. Note that in the chirp case,  $U_4$  is in fact a submatrix  $U_4$ , which can be chosen with only a small number of columns taken away from  $U_4$ . Then, the expectation  $\mathsf{E}_{\pi}[||\Phi x||_2^2]$  based on this choice of the phase factors is shown in the following lemma.

- Lemma 3.2. For the submatrix defined above,  $\Phi = \begin{bmatrix} U_1 & -U_2 & U_3 & -U_4 \end{bmatrix}$ ,
- $\sum_{\ell} \phi_j(\ell) = 0$  for all  $1 \le j \le n$ ,  $\mathsf{E}_{\pi} \left[ \sum_{\ell} \left\langle \phi_j(\ell), \phi_{j'}(\ell) \right\rangle \right] = -\frac{1}{\sqrt{n}} \frac{n}{N-1}$  for all  $j \ne j'$ .

*Proof.* The row sum of  $U_1$  is zero for each row except for the first because all entries in the first row are  $1/\sqrt{n}$  by construction. Consequently, the row sums of  $U_t$ , for t = 2, 3, 4, are also zero except for the first row, in which all entries are  $1/\sqrt{n}$  as well. Therefore, with the phase factors on  $U_2$  and  $U_4$ , all row sums of  $\Phi$  are equal to zero.

The next step is to find the expected inner product between any pair  $\phi_i$  and  $\phi'_i$  with  $j \neq j'$ . For each column  $\phi_j$  from  $U_1$ , the collection formed by pointwise multiplication with the complex conjugate of all other columns of  $\Phi$  except with itself is  $\tilde{\Phi} = \begin{bmatrix} \tilde{U}_1 & -U_X & U_Y & -U_Z \end{bmatrix}$ for some chirp rates X, Y, and Z.  $\tilde{U}_1$  is the same as  $U_1$  but without the first column. Even though X, Y, and Z may not come from chirp rates of  $\Phi$ , they do exist because of (p2). Therefore, the row sum for each row of  $\tilde{\Phi}$  is  $-1/\sqrt{n}$ . Similarly, for each column from  $U_2, U_3$ , or  $U_4$ , the row sum of the collection of the inner products is also  $-1/\sqrt{n}$ . Therefore,

(3.6) 
$$\mathsf{E}_{\pi}\left[\sum_{\ell} \left\langle \phi_j(\ell), \phi_{j'}(\ell) \right\rangle\right] = \frac{N\frac{-1}{\sqrt{n}}}{N(N-1)} = -\frac{1}{\sqrt{n}}\frac{n}{N-1},$$

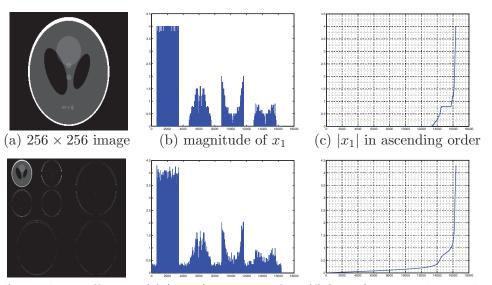
because there are 4n = N columns in  $\Phi$  and the total number of inner products is 4n(4n-1) =N(N-1).

Lemma 3.1 can now be proved using Lemma 3.2, and thus the following result holds for submatrices.

Theorem 3.3. If a submatrix has the form  $\Phi = \begin{bmatrix} \alpha_1 U_1 & \alpha_2 U_2 & \cdots & \alpha_J U_J \end{bmatrix}$ , where  $\alpha_1, \ldots, \alpha_J U_J = \begin{bmatrix} \alpha_1 U_1 & \alpha_2 U_2 & \cdots & \alpha_J U_J \end{bmatrix}$  $\alpha_J$  are real- or complex-valued scalars with  $|\alpha_i| = 1$  and  $\alpha_1 + \cdots + \alpha_J = 0$ , then  $\Phi$  satisfies  $(k, \varepsilon, \delta)$ -UStRIP, with  $\delta$  described in (2.5).

As noted earlier, in some cases considered in this paper the signal length is not an integer multiple of n, and it is necessary to remove a small number s of columns from  $U_J$  to make a sensing matrix of suitable size. The expected value of the component of a uniformly distributed k-sparse unit N-vector falling in the s-dimensional subspace defined by the deleted columns is less than  $s^2/N \ll 1$ , so the StRIP condition (2.4) will still be satisfied in this case with slightly less favorable  $\varepsilon$ .

**3.3.** Initial best approximation. This section proposes a new approach for detecting a large portion of the nonzero locations in one step. The approach is based on the observation that many important classes of images, including medical images, are low-pass in nature. Consequently, most of their energy is captured by the coarse-scale wavelet coefficients (i.e., in the upper-left region of a multiscale analysis diagram). This general structure can be exploited without more explicit a priori knowledge of individual images. Although the idea is explained



(d) wavelet coefficients (e)  $|U_{P_1}^*y|$ : approx. of  $x_1$  (f)  $|U_{P_1}^*y|$  in ascending order

**Figure 1.** (a) is the standard Shepp-Logan image, and (d) demonstrates that the energy of wavelet coefficients is concentrated in the upper-left region. (b) shows the absolute value of  $x_1$  entries, and (c) is the plot of  $|x_1|$  sorted in the ascending order. Similarly, (e) shows the magnitude of  $|U_{P_1}^*y|$ , and then (f) orders  $|U_{P_1}^*y|$  in the ascending order. Comparing (c) and (f), it follows that  $|U_{P_1}^*y|$  approximates  $|x_1|$  well.

here in the context of the RM sensing matrix, the same concept works for the chirp sensing matrix as well. The measurements can be written as

(3.7) 
$$\Phi x = \begin{bmatrix} U_{P_1} & U_{P_2} & U_{P_3} & U_{P_4} \end{bmatrix} \begin{vmatrix} x_1 \\ x_2 \\ x_3 \\ x_4 \end{vmatrix} = U_{P_1} x_1 + U_{P_2} x_2 + U_{P_3} x_3 + U_{P_4} x_4,$$

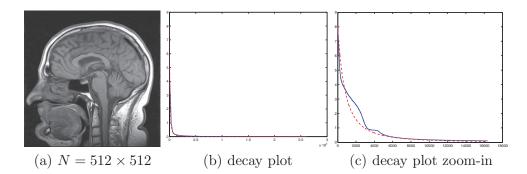
where  $x_1, x_2, x_3$ , and  $x_4$  are vectors of the upper-left, lower-left, upper-right, and lower-right coefficients, respectively. It is possible to estimate  $x_1$  by

(3.8) 
$$U_{P_1}^* y = x_1 + U_{P_1}^* U_{P_2} x_2 + U_{P_1}^* U_{P_3} x_3 + U_{P_1}^* U_{P_4} x_4$$

where \* denotes the conjugate transpose. The last three terms are small because  $x_2, x_3$ , and  $x_4$  are much sparser and smaller than  $x_1$ , and, furthermore,  $U_{P_1}^* U_{P_2}, U_{P_1}^* U_{P_3}$ , and  $U_{P_1}^* U_{P_4}$  are small as well, as discussed in section 3.1. Therefore,  $U_{P_1}^* y \approx x_1$ . In the case when all nonzero locations are in the upper-left region, i.e.,  $x_2, x_3$ , and  $x_4$  are zero,  $U_{P_1}^* y$  is equal to  $x_1$ , which automatically completes the image reconstruction.

Figure 1 shows an example of this method with an RM sensing matrix, where (a) is the Shepp-Logan phantom image of pixel resolution  $256 \times 256$  and (d) shows its Haar wavelet coefficients. From (b) and (e), it is evident that  $U_{P_1}^* y$  is a good approximation of  $x_1$  (with added cross-terms in  $U_{P_1}^* y$  from the last three terms of (3.8)). The nonzero locations in  $x_1$  are then found by thresholding.

The threshold is determined by the following method. First,  $|U_{P_1}^*y|$  is sorted in ascending order, as shown in Figure 1(f). Observe that the graph in (f) is a smooth version of the



**Figure 2.** (a) is the initial MRI image; in (b) the blue solid curve represents the absolute values of the wavelet coefficients of image (a) in the descending order. The red dashed curve approximates the blue curve quite well and is (3.10) with s = 2,  $H = 400 \frac{N}{216}$ , and Const = maximum absolute values of wavelet coefficients.

graph in (c). The threshold is picked as the critical point<sup>1</sup> closest to the origin. In (f), such a critical point is around 14000. Denoting the detected locations by  $(P_l, b_l)$ ,  $l = 1, \ldots, t$ , the magnitudes  $z_l$  can be well estimated by solving the least-squares problem,  $\min_z ||Az - y||$ , where A is the matrix whose columns consist of  $\phi_{P_l,b_l}$  and  $z = [z_1, \ldots, z_t]^T$ . The solution is  $z_{sol} = (A^*A)^{-1}A^*y$ . Since  $P_l = P_1$  in the initial step and  $U_{P_1}$  is orthogonal, the solution is  $z = A^*y$ . This is the *initial best approximation*.

This method entails low computational cost, since it requires only one length-n FFT or FHT and sorting of one n-vector. Empirically, the initial best approximation step already gives small reconstruction error, around -18 dB, where the error is defined as

(3.9) 
$$\operatorname{Error}(\mathrm{dB}) = 10 \log_{10} \left[ \frac{||x_{\mathrm{actual}} - x_{\mathrm{reconstructed}}||^2}{||x_{\mathrm{actual}}||^2} \right]$$

Note that the negative of the above error is known as the signal-to-noise ratio.

*Error estimation.* To estimate the error of the initial approximation method, the coefficients of x are arranged in decreasing order,  $|x_{(1)}| \ge |x_{(2)}| \ge \cdots \ge |x_{(N)}|$ . Assume that the wavelet coefficients have the following decay property (this is consistent, for example, with [20, 12]):

(3.10) 
$$|x_{(n)}| \approx \operatorname{Const} \cdot (n+H)^{-s}$$

for some  $s \ge 1$  and H > 0. Figure 2 shows and example of an MRI image and its wavelet coefficients in the decreasing order, which fit well with (3.10). The approximation of ||x|| is given by

$$(3.11) ||x||_{2} = \left\|\sum_{n=1}^{N} x_{(n)}\phi_{(n)}\right\|_{2} = \sqrt{\left|\sum_{n=1}^{N} x_{(n)}\phi_{(n)}\right|^{2}} \approx \sqrt{\sum_{n=1}^{N} \left|x_{(n)}\right|^{2}} \approx \operatorname{Const} \sqrt{\sum_{n=1}^{N} (n+H)^{-2s}}.$$

<sup>1</sup>In the continuous case it would be exactly the critical point, i.e., where the derivative does not exist; however, this is a discrete setting, and so the term "critical point" is used loosely.

If the largest M coefficients are detected, the error between the initial best approximation  $x_M = \sum_{n=1}^M x_{(n)}\phi_{(n)}$  and the actual x is

(3.12) 
$$||x_M - x||_2 = \left\|\sum_{n=M+1}^N x_n \phi_{(n)}\right\|_2 \approx \text{Const} \cdot \sqrt{\sum_{n=M+1}^N (n+H)^{-2s}}.$$

Therefore, the error of this initial approximation method is about

(3.13) 
$$\operatorname{Error_{init}} \approx 10 \log_{10} \left[ \frac{\sum_{n=M+1}^{N} (n+H)^{-2s}}{\sum_{n=1}^{N} (n+H)^{-2s}} \right].$$

For example, let N be the image size and suppose that the largest 2% coefficients are detected, i.e., M = 2% of N. The wavelet coefficients of several images are described by the decay (3.10) with s = 2 and  $H = 400 \frac{N}{2^{16}}$ . Then for  $N = 256^2, 512^2$ , and  $1024^2$  the calculation of (3.13) gives the initial error

$$\text{Error}_{\text{init}} \approx -18.9 \text{ dB}.$$

**3.4. Detecting nonzero locations with DCFT and DCHT.** The discrete chirp Fourier transform (DCFT) of an *n*-point signal x, defined in [35], can be written as

(3.14) 
$$X_c(r,m) = \frac{1}{\sqrt{n}} \sum_{\ell=0}^{n-1} x(\ell) (W_n)^{r\ell^2 + m\ell},$$

where  $W_n = e^{-2\pi i/n}$ . The discrete chirp Hadamard transform (DCHT) is defined analogously; and for brevity, only the case of DCFT is shown in this section. In the above definition, r and m are the chirp rate and frequency, respectively. For a fixed  $r_t$ ,

(3.15) 
$$X_c(r_t, m) = \frac{1}{\sqrt{n}} \sum_{\ell=0}^{n-1} x(\ell) (W_n)^{r_t \ell^2 + m\ell}.$$

Defining

(3.16) 
$$x_{r_t}(\ell) = x(\ell)(W_n)^{r_t\ell^2},$$

yields

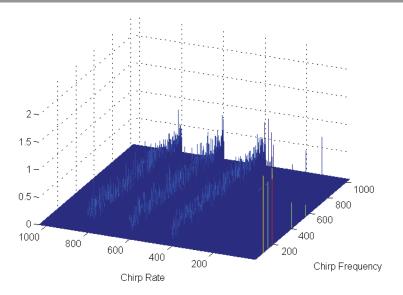
(3.17) 
$$X_c(r_t, m) = \operatorname{DFT}_n \left\{ x_{r_t}(\ell) \right\}, \quad t = 1, 2, 3, 4.$$

Note that only four *n*-point DFTs (discrete Fourier transform) need to be evaluated, since only four chirp rates are used. Of the 4n DCFT coefficients computed, the ones with largest absolute values are chosen. The corresponding (r, m) pairs from the DCFT plane (see Figure 3) are used to recover the chirp sensing matrix columns. In this setting, applying the DCFT to detect nonzero locations is the same as dechirping with all four chirp rates and then applying the DFT:

(3.18) 
$$w(r_t, \ell) = \operatorname{DFT}_n \left\{ y_0(\ell) \overline{\Phi_{r_t,0}(\ell)} \right\}, \quad t = 1, 2, 3, 4.$$

The first d largest coefficients  $|w(r_t, \ell)|$  are then selected, giving d pairs  $(r_t, \ell)$ . In the experiments presented in section 4.2,  $d \approx 100$ .

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**Figure 3.** DCFT plane: chirp rate  $r_t$  versus chirp frequency. Here, only four rates in  $X_c$  from (3.17) are relevant:  $r_1 = 0, r_2 = 200, r_3 = 400, r_4 = 800$ ; the height here is  $|X_c|$ .

This selection procedure can be visualized as follows. The DCFT plane is an  $n \times n$  plane for an *n*-point signal. For the Shepp-Logan phantom image of  $64 \times 64$  size and 1% sparsity the DCFT plane is shown in Figure 3. The chirp rate axis has only four points per frequency cycle due to the selection of only four chirp matrices (in the example, the rates are 0, 400, 600, 800), while the chirp frequency axis is dense due to the true nonzero coefficients from the sparse signal as well as from the side-lobes introduced during the dechirping step.

**3.5. Updated pseudoinverse solution.** The third step finds the values  $z_t$  by solving the linear least-squares problem

$$(3.19) \qquad \qquad \min_{z} \left\| Az - y \right\|,$$

where A is a submatrix of the sensing matrix and  $z = [z_1, \ldots, z_t]^{\mathsf{T}}$  is a vector. Two methods are proposed for this step. This section describes the first method, while the second method is discussed in the next subsection.

Note that the matrix A in the current step can be expressed as  $A = \begin{bmatrix} \widetilde{A} & c \end{bmatrix}$ , where  $\widetilde{A}$  is the matrix in the previous least-squares problem and c is the newly found column. To solve these least-squares problems without treating each problem (iteration) independently, it is possible to use an updated pseudoinverse solution method whose computation is based on previous calculations. The pseudoinverse solution of (3.19) is

(3.20) 
$$z_{sol} = (A^*A)^{-1}A^*y.$$

The inverse of

(3.21) 
$$A^*A = \begin{bmatrix} \widetilde{A}^*\widetilde{A} & \widetilde{A}^*c \\ c^*\widetilde{A} & c^*c \end{bmatrix}$$

can be computed efficiently by the Schur-Banachiewicz blockwise inversion formula [6]:

(3.22) 
$$\begin{bmatrix} D & E \\ F & G \end{bmatrix}^{-1} = \begin{bmatrix} D^{-1} + D^{-1}EVFD^{-1} & -D^{-1}EV \\ -VFD^{-1} & V \end{bmatrix}$$

where  $V = (G - FD^{-1}E)^{-1}$ . Since  $D^{-1} = (\widetilde{A}^*\widetilde{A})^{-1}$  is known from the previous iteration and the size of  $V = (G - FD^{-1}E)^{-1}$  is small, the calculation is very efficient. The calculation of  $A^*y$  can be done using previous steps by

(3.23) 
$$A^*y = \begin{bmatrix} \tilde{A}^*y \\ c^*y \end{bmatrix},$$

where the size of c is much smaller than the size of A.

3.6. Fast methods for DCFT and DCHT with an arbitrary subset of columns. The second method for solving the least-squares problem (3.19) is by the LSQR algorithm of Paige and Saunders [31], replacing the above pseudoinverse solution approach. The LSQR algorithm is an efficient iterative method for solving the least-squares problem if the matrix A is sparse or the matrix-vector multiplications by A and  $A^*$  can be done efficiently. Therefore, this section begins by showing how to efficiently apply  $\Phi$  and  $\Phi^*$  to length-N and length-n vectors, respectively, without directly calculating matrix-vector products. Subsequently, an efficient method for multiplying A and  $A^*$  is described, where A is an arbitrary submatrix of  $\Phi$ , formed by concatenating a set of columns of  $\Phi$ .

First, write the matrix multiplication  $\Phi x$  as the blockwise matrix multiplications:

$$\Phi x = \begin{bmatrix} U_1 & U_2 & U_3 & U_4 \end{bmatrix} \begin{bmatrix} x_1 \\ x_2 \\ x_3 \\ x_4 \end{bmatrix}$$
(3.24)

Recall that  $U_1$  is the discrete inverse Fourier or Walsh–Hadamard transform, up to a scaling. A key step here is to express  $U_t$  for  $t \neq 1$  as the product of a diagonal matrix  $D_{v_t}$  with diagonal  $v_t = \phi_{r_t,0}$  or  $v_t = \phi_{P_t,0}$  and matrix  $U_1$  as follows:

$$(3.25) U_t = D_{v_t} U_1$$

Then,

$$(3.26) (D_{v_t}U_1) x_t = D_{v_t} (U_1 x_t).$$

Therefore, instead of directly multiplying the matrix  $U_t$  with  $x_t$ , one can first apply the inverse fast Fourier (or Walsh–Hadamard) transform to  $x_t$  and then carry out pointwise vector-vector multiplication of  $v_t$  and  $U_1x_t$ . So,  $\Phi x$  in (3.24) can be calculated with only four FFTs or FHTs.

The calculation of Az can be efficiently carried out by a slight modification of the above method for  $\Phi x$ . Consider a length-N zero vector  $x_z$ . The coefficients of z are inserted at those locations in  $x_z$  that correspond to the columns of  $\Phi$  that make up the matrix A. Then,  $Az = \Phi x_z$  can be efficiently calculated as described above. For efficient calculation of  $\Phi^* y$ , one can start by expressing it as a blockwise matrix multiplication:

(3.27) 
$$\Phi^* y = \begin{bmatrix} U_1^* \\ U_2^* \\ U_3^* \\ U_4^* \end{bmatrix} \begin{bmatrix} y \\ y \\ U_2^* \\ U_3^* \\ U_4^* \end{bmatrix} = \begin{bmatrix} U_1^* y \\ U_2^* y \\ U_3^* y \\ U_4^* y \end{bmatrix}.$$

Therefore,  $\Phi^* y$  can be obtained by concatenating four vectors  $U_t^* y$ , for t = 1, 2, 3, 4, into a long vector. The matrix  $U_1^*$  is the Fourier matrix or the Walsh–Hadamard matrix. Each  $U_t^*$  can be written as the product of  $U_1^*$  and  $D_{\overline{v_t}}$ , where  $D_{\overline{v_t}}$  is a diagonal matrix with diagonal  $\overline{v_t}$ :

$$(3.28) U_t^* = U_1^* D_{\overline{v_t}} .$$

Using this expression for  $U_t^* y$ , the calculation can be carried out by applying the fast Fourier or Walsh–Hadamard transform after the pointwise vector-vector multiplication of  $\overline{v_t}$  and y:

(3.29) 
$$U_t^* y = (U_1^* D_{\overline{v_t}}) y = U_1^* (D_{\overline{v_t}} y).$$

Finally, the calculation of  $A^*y$  can be efficiently carried out by a slight modification of the method for  $\Phi^*y$ . First, calculate  $\Phi^*y$  as above and get a length-N vector, say x. Then, from x, choose only the positions that have corresponding columns in A to form a length-j vector,  $x_A$ . This is because  $A^*$  is a submatrix of  $\Phi^*$  with selected rows from  $\Phi^*$ . Therefore,  $A^*y$  can also be efficiently calculated.

Using these efficient methods, the least-squares problem (3.19) may be solved via an LSQR algorithm instead of the updated pseudoinverse solutions method of section 3.5.

**3.7. Three versions of the reconstruction algorithm.** This section describes how the features introduced in the preceding sections are incorporated into the image reconstruction algorithm. The reconstruction algorithm is built up step-by-step with the most efficient reconstruction (called version 3, or v3), with the goal of comparing how each modification improves the reconstruction.

Version 1 (v1) consists of three iterative steps: detecting the nonzero locations, finding the corresponding coefficients, and getting the residuals. These steps are repeated until the residual is sufficiently small. Specifically, nonzero location detection is done using DCFT or DCHT as described in section 3.4 instead of using the shift-and-multiply method and then applying FFT or FHT [2, 25]. Since only a few chirp rates are used, multiple nonzero locations can be found in each iteration of the algorithm. Then, v1 uses the updated least-squares method with the pseudoinverse solution, as described in section 3.5, to find the coefficients without treating each iteration independently. This method was applied with the chirp sensing matrix in [30].

In version 2 (v2), the initial approximation step explained in section 3.3 is added before the iterative steps to detect a significant number of the nonzero coefficients. This was applied with the RM matrix in [29]. The additional approximation step speeds up the algorithm, and, more importantly, the reconstruction fidelity is improved when the image sparsity is increased.

# Step 0: approx.Step 1: detectionStep 2: least-squaresv1noDCFT or DCHT sect. 3.4Updated pseudoinverse solutions sect. 3.5v2sect. 3.3DCFT or DCHT sect. 3.4Updated pseudoinverse solutions sect. 3.5v3sect. 3.3DCFT or DCHT sect. 3.4LSQR with fast DCFT or DCHT sect. 3.6

Table 2Three versions of algorithms.

Note that, as discussed in section 3.3,  $x_2$ ,  $x_3$ , and  $x_4$  are assumed to be much sparser than  $x_1$  when the initial approximation is used.

The v3 algorithm also incorporates the initial approximation step. The improvement comes largely from the reconstruction time and storage in the second iterative step. Now the coefficients are found by using the fast DCFT or DCHT method introduced in section 3.6 along with the LSQR algorithm for solving the least-squares problem.

The comparison is given in Table 2 with the following steps in each version:

- Step 0: approximation of the solution,
- Step 1: detection of nonzero locations,
- Step 2: finding the coefficients using least-squares,
- Step 3: getting the residual and repeating steps 1 and 2 if the residual is not sufficiently small.

Algorithm v3.

Input:  $y, \Phi = \begin{bmatrix} U_1 & -U_2 & U_3 & -U_4 \end{bmatrix}$ Output:  $\tilde{z}$ 

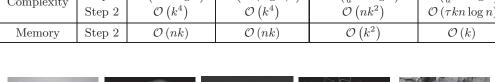
- 0. Approximation: Perform hard-thresholding  $U_1^*y$  to obtain a set of nonzero locations, denoted by  $\Gamma$ . Let  $A = U_1|_{\Gamma}$  be a submatrix of  $U_1$  restricted on the set  $\Gamma$ . Then, the initial approximation is  $\tilde{z} = A^*y$ , and the residual is obtained by  $y_0 = y A\tilde{z}$ .
- 1. Detection: From  $w(t, \ell) = DFT_n\{y_0(\ell)\overline{v_t(\ell)}\}, t = 1, 2, 3, 4$ , where DFT is DHT in the RM case and  $v_t$  is the first column of  $U_t$ , update  $\Gamma = \Gamma \cup \{\text{locations associated with } d \text{ largest } |w(t, \ell)|\}$ . Let  $A = \Phi|_{\Gamma}$ .
- 2. Least-squares:  $\tilde{z} = \operatorname{argmin}_{z} \|y Az\|_{2}$ .
- 3. Define  $y_0 = y A\tilde{z}$ . Repeat steps 1–3 until  $||y_0||_2$  is sufficiently small.

4. Performance analysis and experiments. In this section, the performance of the approach described in the preceding section is analyzed in terms of computational complexity and memory use. Results from a number of experiments involving both natural scene and medical images are also summarized.

**4.1. Computational complexity and memory.** The chirp quadratic reconstruction algorithm (QRA) detects the nonzero locations one-by-one with n-1 length-n FFTs. Therefore, the total computational complexity for Step 1 is  $\mathcal{O}(kn^2 \log n)$ . For RM QRA,  $p \ (= \log n)$  length-n FHTs are used for nonzero location detection. The computational complexity is thus  $\mathcal{O}(kn(\log n)^2)$ . For QRA with both chirp and RM, Step 2 uses a pseudoinverse method to solve the least-squares problem. Specifically, since the matrix A is of size  $n \times t$ , n > t, this is usually done with the QR factorization. Therefore, the overall computational complexity is  $\mathcal{O}(\sum_{t=1}^{k} t^3) = \mathcal{O}(k^4)$ . Consequently, if the sparsity k is significantly small (i.e.,  $k \ll n \ll N$ ), this method is very efficient. However, when k is not so small, which is usually the case

		Chirp QRA	RM QRA	Chirp/RM v1/v2	Chirp/RM v3
Complexity	Step 1	$\mathcal{O}\left(kn^2\log n\right)$	$\mathcal{O}\left(kn(\log n)^2\right)$	$\mathcal{O}\left(\frac{1}{d}kn\log n\right)$	$\mathcal{O}\left(\frac{1}{d}kn\log n\right)$
Complexity	Step $2$	$\mathcal{O}\left(k^4 ight)$	$\mathcal{O}\left(k^{4} ight)$	$\mathcal{O}\left(nk^{2} ight)$	$\mathcal{O}\left(\tau kn\log n\right)$
Memory	Step 2	$\mathcal{O}\left(nk ight)$	$\mathcal{O}\left(nk ight)$	$\mathcal{O}\left(k^2 ight)$	$\mathcal{O}\left(k ight)$

Table 3 Computational complexity of each step for different versions of the algorithm.



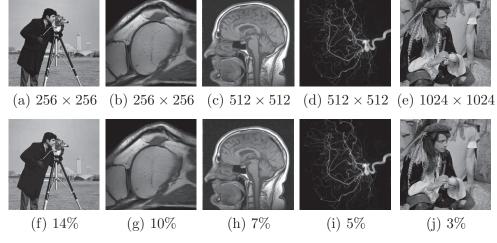


Figure 4. Top row shows original images. Bottom row shows the sparsified images.

for real images, it becomes inefficient. For chirp and RM algorithms v1, v2, and v3, Step 1 uses only a few (for example, 4) length-n FFTs or FHTs to detect d nonzero locations in one iteration. Therefore, the total computational complexity is  $\mathcal{O}(\frac{1}{d}kn\log n)$ . In all the experiments presented here, d = 100. For chirp and RM, in both v1 and v2, Step 2 uses the updated pseudoinverse method to find the nonzero coefficients, wherein multiplications with the matrix A of size  $n \times t$  are carried out. Therefore, the overall computational complexity is  $\mathcal{O}(\sum_{t=1}^{k} nt) = \mathcal{O}(nk^2)$ . The memory is  $\mathcal{O}(k^2)$  because  $(A^*A)^{-1}$  needs to be stored and has size  $t \times t$ . In Step 2 of chirp and RM for v3, because of the use of the fast DCFT or DCHT algorithms that need a few length-n FFTs or FHTs, the total computational complexity is  $\mathcal{O}(\tau kn \log n)$ , where  $\tau$  is the iteration number of convergence. The memory cost in this case is only  $\mathcal{O}(k)$  because only the t chirp-frequency pairs related to the matrix A need to be stored. The comparison is given in Table 3.

**4.2.** Experimental results and comparisons. For the experiments, each original image was sparsified by computing its Haar wavelet transform and then retaining a predetermined fraction of its wavelet coefficients, keeping the largest coefficients and setting the rest to zero. The image data were compressively sensed (measured) with chirp, RM, and noiselet matrices of the same size (for chirp, the closest prime number) and then reconstructed by their respective algorithms. Figure 4 shows the original images with sizes ranging from  $256 \times 256$  to  $1024 \times 1024$ and their corresponding sparsified images with the predetermined sparsity.

Table 4

Reconstruction errors and times from experiments with all three versions of chirp compressed sensing.

	Chirp v1		Chirp v2		Chirp v3	
	error	time	error	time	error	time
Cameraman, $256 \times 256$ , $14\%$	-239  dB	7.3 h	-249  dB	12 h	-109  dB	$28 \mathrm{s}$
Knee, $256 \times 256$ , $10\%$	-245  dB	152 m	-260  dB	80 m	-119  dB	$7 \mathrm{s}$

#### Table 5

Reconstruction errors and times from experiments with all three versions of RM compressed sensing.

	RM v1		RM v2		RM v3	
	error	time	error	time	error	time
Cameraman, $256 \times 256$ , $14\%$	failed	-	failed	-	$-43.7~\mathrm{dB}$	$33 \mathrm{s}$
Knee, $256 \times 256$ , $10\%$	failed	-	-284  dB	31 m	-108  dB	$18 \mathrm{~s}$

Table 4 shows the reconstruction errors and times for all three versions of the chirp reconstruction algorithm. Note that the experiments were done in MATLAB and the codes are not optimized, so run-time comparisons should be interpreted accordingly. For reconstruction fidelity, v2 is slightly better than v1. Table 5 shows the reconstruction errors and times for all three versions of the RM reconstruction algorithm. For reconstruction fidelity, v2 is much better than v1 because the initial approximation step is able to correctly detect a large number of nonzero locations. Among all experiments performed (including many not shown in the tables), the highest sparsity level for which chirp  $v^2$  and RM  $v^2$  were able to accurately reconstruct is larger than that for chirp v1 and RM v1. In terms of reconstruction time, v3 is better than v2 because v3 uses the fast DCFT or DCHT method to find the coefficients. In the table, s, m, and h stand for seconds, minutes, and hours, respectively. The reconstruction results by chirp v3 and RM v3 are better than those of the other versions. The error is about -110 dB, which is larger than the error for v2 because v2 directly computes the closed-form solution of the least-squares problem and v3 approaches the solution iteratively. The reconstructed images by chirp v1, v2, and v3 in Table 4 are shown in Figure 5, in which all the reconstructed images look essentially identical to the reference images.

Table 6 and Figure 6 show experimental results obtained with chirp v3 and RM v3 algorithms, with a comparison to the results of using random noiselet measurements with  $\ell_1$ minimization. A real-valued noiselet transform is used (fast code provided by Romberg) and YALL1 [36] is used for  $\ell_1$ . Note that Candès and Romberg have used noiselets for compressed sensing in [10]. The measurements are again operated on the wavelet domain of each sparsified image. The reference images with predetermined sparsities are shown in column (a). The reconstructed images by noiselets, chirp, and RM are shown in columns (b), (c), and (d), respectively. The results of column (c) are by chirp v3 algorithm and of (d) are by RM v3 algorithm. Both chirp v3 and RM v3 provide better reconstruction fidelity than reconstruction using random noiselet measurements.

Finally, Table 7 shows experimental results using the original unsparsified images. The reconstruction errors obtained with the chirp v3 and RM v3 algorithms are better than those obtained by using random noiselet measurements. This supports the practicality of the proposed methods directly on real images.

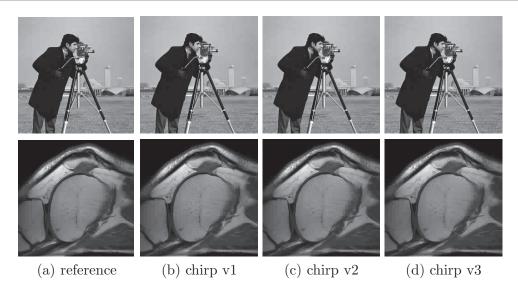


Figure 5. Reconstructed images with chirp v1, v2, and v3 look merely identical to the (sparsified) reference images.

Image	n/N	Noiselets	Chirp v3	RM v3
size, sparsity				
Brain	25%	-25.2  dB	-123  dB	-119  dB
$512 \times 512, 7\%$				
Vessel	25%	-38.9  dB	-129  dB	-125  dB
$512 \times 512, 5\%$				
Vessel	12.5%	-10.1  dB	$-49.9~\mathrm{dB}$	-10.6  dB
$512 \times 512, 5\%$				
Man	6.25%	-14.5  dB	-112  dB	-109  dB
$1024 \times 1024, 2.38\%$				

 Table 6

 Reconstruction error using noiselets, chirp v3, and RM v3 algorithms.

5. Discussion and conclusions. This paper describes an approach to improving the utility of compressed sensing using deterministic matrices consisting of chirps or second-order RM codes. Specifically, we discuss a reconstruction algorithm and some variations that extend the utility of the algorithms described in [2] and [25] to less sparse signals and, in particular, images. Several examples illustrating the performance of this approach with images with varying modest degrees of sparsity and having different characteristics in other respects are also presented.

We believe it is likely possible to make further improvements in both reconstruction efficiency and accuracy using chirps and RM codes in compressed sensing of signals having limited sparsity by improving the process of peak detection entailed in identifying the locations of nonzero values in the sparse signal.

Although they are designed for compatibility with the reconstruction approach discussed in this paper, it would be possible to use the sampling matrices constructed here with other reconstruction methods (e.g., directly with basis pursuit). We have not looked into this either

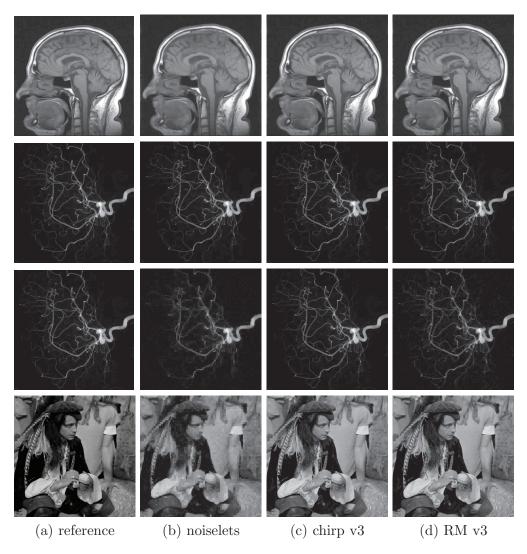


Figure 6. Reconstructed images with noiselets, chirp, and RM corresponding to Table 6.

Image Noiselets Chirp v3  $\rm RM~v3$ n/Nsize Brain 25% $-23.4~\mathrm{dB}$ -28.4 dB-25.7 dB $512\times512$ Vessel 25%-12.0 dB-14.1 dB $-15.4~\mathrm{dB}$  $512\times512$ Man 25% $-20.0~\mathrm{dB}$ -23.2 dB $-22.6~\mathrm{dB}$  $1024\times1024$ 

 Table 7

 Reconstruction error using noiselets, chirp v3, and RM v3 algorithms. The images are not sparsified.

analytically or experimentally, though it would be of interest to see how well they perform compared to random matrices using other reconstruction schemes.

Additionally, it is noted that the method used here, although applied to images, is essentially one-dimensional. Ongoing work is investigation of more natural formulations for multidimensional signals. Finally, the set of RM codes is naturally partitioned into a hierarchy of subfamilies, beginning with the Kerdock codes that have very good correlation properties and continuing through Delsarte–Goethals families in which the inner product magnitudes between codes increase according to orderly bounds. It may be possible to exploit this structure in the compressed sensing process, particularly when some a priori information is available about the distribution of the locations of the nonzero components. This is often the case with images, many classes of which are known to possess a low-pass structure in addition to being compressible in certain bases (e.g., wavelets). They admit approximations that not only are somewhat sparse, but in which the locations of the nonzero coefficients are not uniformly distributed.

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